



Fluoroscopic and tomographic correlation for aortic annulus measurements in transcatheter aortic valve implantation: “follow the right cusp” rule

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ABSTRACT

Introduction and objectives: Coronary computed tomography angiography (CCTA) has become the gold standard to measure the size of the aortic annulus and better select the size of transcatheter heart valves (THV) in patients undergoing transcatheter aortic valve implantation (TAVI). However, in selected cases, CCTA may not be feasible. Angiographic aortic annulus (AAA) measurements during TAVI may be an alternative and should be evaluated for precision regarding the proper selection of THV sizes. We sought to investigate the correlation between AAA and CCTA measurements for the proper selection of balloon-expandable valve (BEV) sizes in patients undergoing TAVI.

Methods: Patients undergoing TAVI with BEV and high-quality CCTA were included. AAA measurements were obtained in the standard 3-cusp view after aortic root aortography. Angiographic distance between non- and left coronary cusps were compared to CCTA annulus measurements. Endpoints were diagnostic tests and correlations between angiographic and CCTA measurements, and the composite endpoint of the VARC-3-defined efficacy (technical success, correct position, and intended performance), and safety profile (multiple valves, valve embolization, pacemaker implantation, and more than moderate valvular regurgitation).

Results: Regarding the Sapien family of THV, aortography-based distance measurements showed a correlation of 0.528 ($P < .01$), 0.451 ($P < .01$), and 0.579 ($P < .01$) for 23 mm, 26 mm, and 29 mm valves with CCTA-based distance measurements. No difference was seen regarding the VARC-3-defined efficacy (94.2% vs 96.0%; $P = .60$) and safety profile (90.9% vs 91.9%; $P = .84$) among cases showing discordant and concordant pairs of measurements.

Conclusions: AAA measurement showed a moderate diagnostic test and Spearman's correlation coefficient compared to CCTA-based annulus assessment for perioperative THV size selection. This strategy could potentially enable TAVI in patients in whom access to preoperative CCTA is not available.

Keywords: non-coronary cusp, left coronary cusp, aortography, angiographic aortic annulus measurements, transcatheter aortic valve implantation.

Correlación fluoroscópica y tomográfica para medir el anillo aórtico en el implante percutáneo de válvula aórtica: regla de la cúspide coronaria derecha

RESUMEN

Introducción y objetivos: La angiografía por tomografía computarizada (angio-TC) es el estándar para medir el anillo aórtico en pacientes tratados mediante implante percutáneo de válvula aórtica (TAVI), aunque en algunos casos podría no ser factible. Debería evaluarse la precisión de la medición del anillo aórtico angiográfica (AAA) durante el TAVI como alternativa para elegir el tamaño correcto de la válvula cardiaca percutánea. Por ello, investigamos la correlación entre las mediciones angiográficas y por angio-TC para elegir el tamaño adecuado de la válvula en pacientes que reciben un TAVI.

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Métodos: Se incluyeron pacientes de TAVI con prótesis de balón expandible y angio-TC de alta calidad. Las mediciones del AAA se obtuvieron de la angiografía de la raíz aórtica en proyección de 3 cúspides. Se comparó la distancia angiográfica entre la cúspide izquierda y no coronaria con las mediciones de angio-TC. Se evaluaron la prueba diagnóstica y la correlación entre las medidas angiográficas y de angio-TC, así como la eficacia (éxito técnico, posición correcta y desempeño intencionado) y la seguridad (múltiples válvulas, embolización, implante de marcapasos e insuficiencia valvular moderada o mayor) definida por VARC-3.

Resultados: Para válvulas con balón expandible de 23 mm, la distancia en la aortografía tuvo una correlación de 0,528 ($p < 0,01$) comparada con las mediciones de angio-TC; para las de 26 mm, la correlación fue de 0,451 ($< 0,01$), y para las de 29 mm fue de 0,579 ($< 0,01$). No hubo diferencia en cuanto a eficacia (94,2 frente a 96,0%; $p = 0,60$) y seguridad (90,9 frente a 91,9%; $p = 0,84$) entre casos con medidas concordantes y discordantes.

Conclusiones: Las mediciones del AAA mostraron un moderado valor de prueba diagnóstica y de correlación Spearman en comparación con la angio-TC para elegir el tamaño de la válvula cardíaca percutánea. Esta estrategia podría permitir un TAVI en situaciones en que la angio-TC no esté disponible.

Palabras clave: Cúspide no coronaria. Cúspide coronaria izquierda. Aortografía. Mediciones angiográficas del anillo aórtico. Implante percutáneo de válvula aórtica.

Abbreviations

BEV: balloon-expandable valve. **CCTA:** coronary computed tomography angiography. **LCC:** left coronary cusp. **NCC:** non-coronary cusp. **TAVI:** transcatheter aortic valve implantation. **THV:** transcatheter heart valve.

INTRODUCTION

During transcatheter aortic valve implantation (TAVI), coronary computed tomography angiography (CCTA) remains the key factor to determine the characteristics of the aortic valve and predefine the size of annular valve prior to the selection of specific transcatheter heart valves (THV).^{1,2} Several CCTA protocols were described to achieve reproducible and reliable aortic annulus measurements.^{3,4} At the same time, transthoracic and transesophageal echocardiographic measurements were used to determine the aortic valve annular size showing good correlation with the gold standard of direct surgical and CCTA-based measurements.^{5,6} However, CCTA showed better image quality acquisition, detailed evaluation of the aortic annulus, and other useful anatomies for transfemoral TAVI (aorto-iliac-femoral vessels)⁷ making CCTA the default strategy for preoperative planning.

Adequate THV size selection is an important factor to prevent patient-prosthesis mismatch and reduce the risk of over- and undersizing and, hence, the increased risk of all cause-mortality and unplanned repeat reintervention.^{6,8,9} While CCTA has been established as the gold standard method for annular sizing pre-TAVI implantation,⁴ an associated risk between radiation exposure and cancer, and contrast media and nephropathy has also been described.^{10,11} Furthermore, in selected cases, CCTA may not be feasible prior to TAVI following emergency clinical indications and/or the patients' unstable conditions.

Aortography-only annular measurement was described as an efficient technique to determine the size of aortic annulus and select the size of the THV.^{12,13} Based on the standard 3-cusp view, the angiographic determination of anatomical dimensions with contrast media (and/or balloon-sizing) can facilitate the identification of proper annular size when CCTA-based sizing is not available.¹⁴⁻¹⁷ Aortography-based measurements have been shown to correlate with direct anatomical preoperative aortic annulus measurements.¹³

Against this background, we sought to investigate whether angiographic aortic valve annular measurements between the non-coronary (NCC) and left coronary cusp (LCC) correlate with CCTA-based

measurements to facilitate proper size selection of the THV in a retrospective, all-comers, single-center cohort of patients undergoing TAVI.

METHODS

Study population

This retrospective, observational analysis evaluated all consecutive patients undergoing transfemoral TAVI following heart team evaluation at the German Heart Center cardiovascular disease unit in Munich, Germany. Transfemoral TAVI was performed using a minimalistic approach¹⁸ in all cases, while THV size selection was left to the operator's discretion based on size chart, CCTA measurements, anatomical factors including calcium distribution and severity, aortic valve annular size, coronary height, and disease.

All patients with native tricuspid calcified aortic valve disease, and available high-quality CCTA for TAVI were included in this study. Procedural information was obtained from a customized database and screened for all patients treated from January 2014 through December 2021 at the German Heart Center in Munich, Germany. During this period, a total of 2500 transfemoral TAVI cases were performed using commercially available balloon-expandable (1865) and self-expanding (635) THVs. Only those who received the SAPIEN 3 or the SAPIEN 3 Ultra (Edwards Lifesciences, United States) balloon-expandable valves (BEV) were included in this analysis.

The study was performed in full compliance with the principles set forth in the Declaration of Helsinki, and all patients gave their written informed consent to undergo the procedure. Ethical approval was obtained from the Technical University of Munich ethical committee under registry no. OBSERVAVI (#525/17). CCTA measurements were performed before THV implantation. Angiographic aortic valve annular measurements between the NCC and LCC were performed offline and documented in the database. The baseline clinical and procedural characteristics (including size of the implanted THV and angiographic aortic regurgitation after implantation), and test lab results were obtained from registry data or the

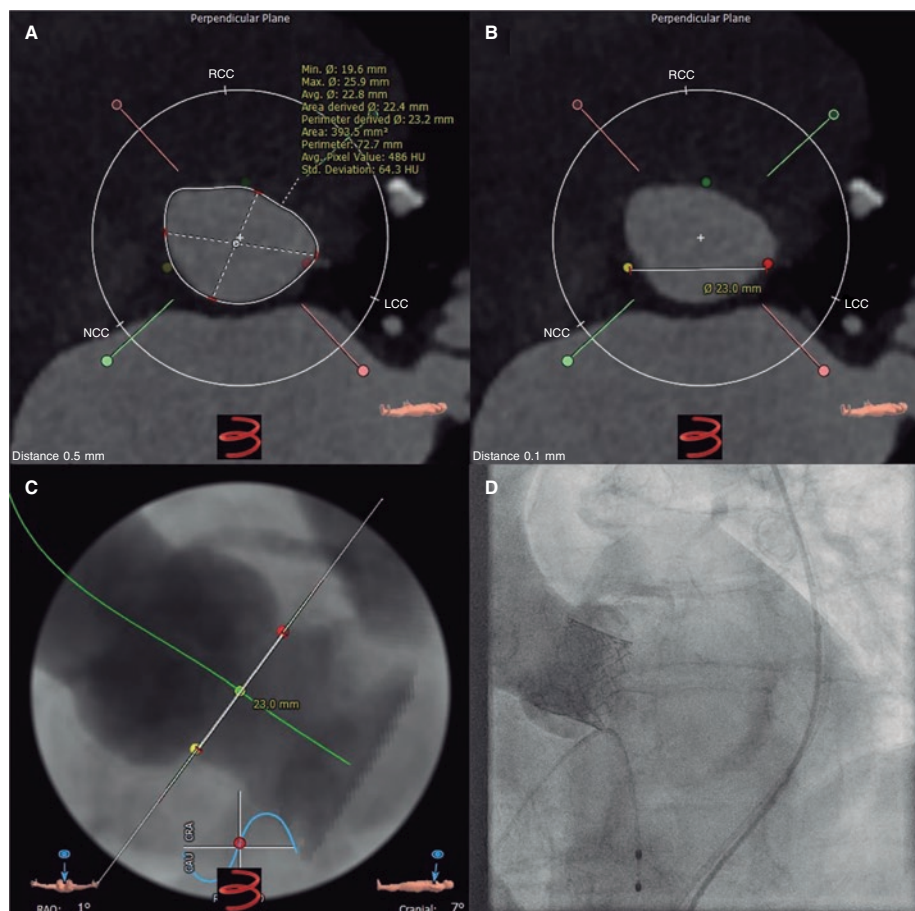


Figure 1. Central illustration. **A:** aortic annulus CTA measurements determining the minimum (19.6 mm), maximum (25.9 mm), and mean (22.8 mm) diameter, perimeter (73 mm), and area (394 mm²). **B:** CTA measurement from the lowest point between the left coronary cusp (red dot) and the non-coronary cusp (yellow dot) with a 23.0 mm distance. **C:** CTA prediction of angiographic angulation to obtain the standard 3-cusp view (cranial right anterior oblique view of first and seventh nerves) with the left-coronary cusp from 1 side (red dot) and the non-coronary cusp on the other side (yellow dot), and the distance between them (23.0 mm). **D:** angiographic result after balloon-expandable valve implantation based on the tomographic measurements shown on figure 1 A (SAPIEN 3 Ultra 23 mm).

clinical records, as appropriate. Regarding the Valve Academic Research Consortium 3 (VARC-3) defined safety and efficacy profile, in-hospital and discharge follow-up was monitored and registered. A 30-day follow-up was established via telephone call, hospital visits or follow-up letter.

Coronary computed tomography angiography measurements

CCTA was analyzed by 1 experienced cardiologist (HA) while a second experienced cardiologist (JM) analyzed a sample of 40 cases to determine inter-observer variability. Using multi-slice computed tomography reconstruction, quantitative measures of the aortic valve annular size (minimum, maximum and mean diameter, perimeter, and area) were obtained based on predefined protocols² using 3-Mensio software (Pie Medical Imaging, The Netherlands). In summary, the 3 hinge points of the aortic cusps were detected and selected. After proper identification of the 3 hinge points, the aortic annulus was seen in automatic multiplanar reconstruction. Annular measurements were obtained 0.5 mm below the hinge points, and the aortic valve annular contour was traced to calculate the perimeter-derived area and diameter (figure 1A). To define the direct one-planar measurement between the NCC and the LCC on the CCTA, a straight line between the red (LCC) and yellow (NCC) hinge points was used to determine length (figure 1B,C). The most

appropriate THV size was selected based on size chart recommendations and anatomical considerations (figure 1D). CCTA-based measurements and calculations were used to determine the proper THV size according to commercial size charts supplied by the manufacturer. The mean diameter and area of the aortic annulus were used to select the THV size (23 mm, 26 mm, and 29 mm) and then coded as a binary variable for each size category; when only 1 measurement was within the proposed range for a specific THV size based on the manufacturer's size chart (within the gray zone), the area was used to decide the final THV size.

Aortographic measurements

All procedures were performed by experienced TAVI operators using a monoplane digital flat panel detector X-ray system (Allura Xper FD 10 C, Royal Philips, The Netherlands) in a dedicated hybrid cath lab. All fluoroscopic 3-cusp view images were analyzed after completion of the procedure and images with distance measurements saved. Angiographic measurements were obtained offline from the angiographic aortic root injection (native annulus without the implanted THV) using a 5-Fr pigtail catheter placed in the right coronary cusp in the standard 3-cusp view.^{14,15} The distance between the NCC and LCC hinge points was measured by experienced cardiologists (HA and JM) using dedicated Phillips

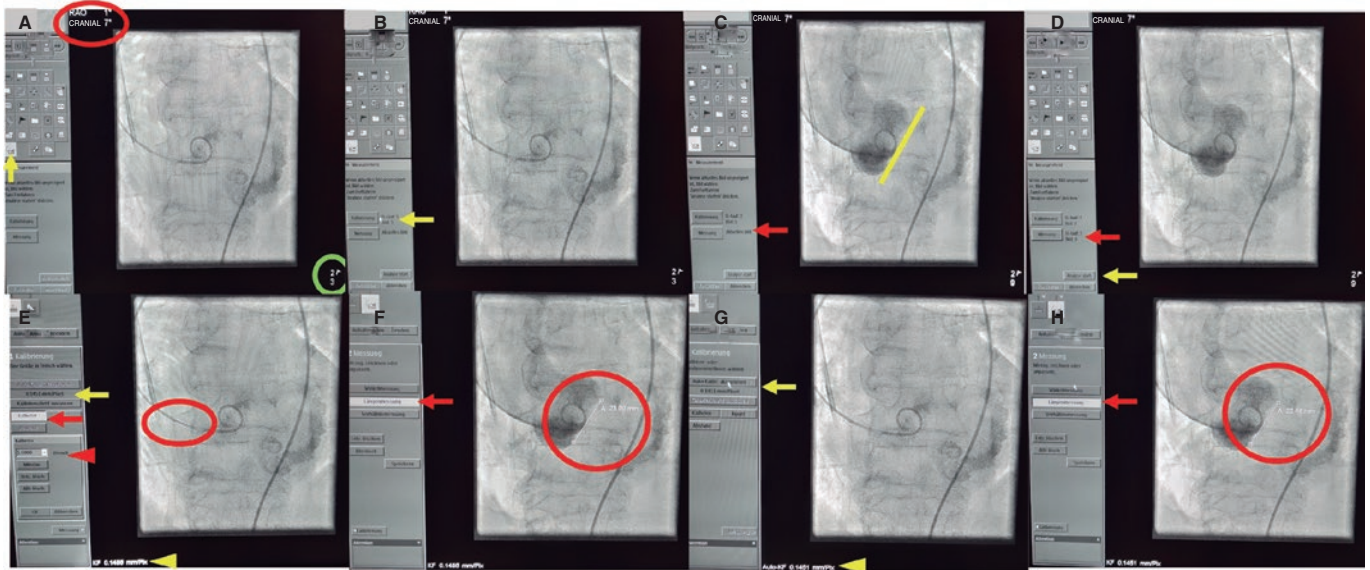


Figure 2. **A:** standard 3-cusp cranial right anterior oblique view of first and seventh nerves (red circle) to determine longitudinal measurement (yellow arrow) in the best contrasted image (green circle). **B:** calibration option based on the best image available (yellow arrow). **C:** measurement option (red arrow) to determine the distance on the aortic annulus (yellow size) on the images saved (green circle). **D:** saved image (red arrow) to “start analysis” (yellow arrow). **E:** manual calibration based on the 5-Fr catheter (red arrow and arrowhead) drawing 2 lines over the catheter (red circle) comparing the calibration factor given by the software (0.1451 mm/pixels, yellow arrow) to the one obtained through manual calibration (0.1486 mm/pixels, yellow arrowhead). **F:** “longitudinal measurement” option should be selected (red arrow) drawing a line at the hinge point of the left and non-coronary cusp (red circle). **G:** for automatic calibration, select “accept automatic calibration” (yellow arrow); the calibration factor given by the software (0.1451 mm/pixels) will be used for measurement purpose (yellow arrowhead, calibration factor of 0.1451 mm/pixels). **H:** aortic valve annulus measurement using automatic calibration selecting “longitudinal measurement” (red arrow) and drawing a line between the hinge points of the left and non-coronary cusp (red circle).

software (figure 2A-H). Angiographic measurements were performed after automatic (based on calibration factor determined by the software) and manual (using the 5-Fr catheter as reference calibration factor) calibration to determine the distance in millimeters.

Endpoints

Endpoints were the correlation between angiographic and CCTA measurements of the distance between the NCC and the LCC. The rates of the VARC-3-defined efficacy (technical success, correct position, and intended performance using VARC-3¹⁹ definitions) and safety profile (multiple valves, valve embolization, pacemaker implantation, and more than moderate valvular regurgitation using VARC-3 definitions) in patients with concordant and discordant measurements between angiographic and CT-based measurements were also analyzed.

Rates of in-hospital complications defined as conversion to surgery, perioperative death, life-threatening bleeding, major and minor bleeding, major and minor vascular complications, and in-hospital mortality in patients with concordant and discordant measurements were reported. The 30-day mortality rate, chronic heart failure, stroke, valve dysfunction, aortic mean gradient, and aortic regurgitation were reported too.

Statistical analysis

Categorical variables were expressed as frequencies and proportions and compared using the chi-square test or Fisher’s exact test, as appropriate. Continuous data were tested for normality with the Shapiro-Wilk test and expressed as mean (\pm standard deviation) or median (interquartile range [IQR]) as appropriate, and then

compared, respectively, using the unpaired *t* test or the Mann-Whitney *U* test.

The study population was divided into derivation ($n = 1256$), and validation cohort ($n = 40$ cases). The study group of interest was obtained from the derivation cohort ($n = 393$). In the derivation cohort, selection of specific THV sizes (23 mm, 26 mm, and 29mm) based on the gold standard CCTA assessment was categorized as a binary variable and then compared to the THV size selection derived from aortography. Subsequently, logistic regression analysis was performed using the binary variable from the CCTA-based THV selection as a dependent variable while aortographic distance measurements were considered an independent variable. Afterwards, the receiver operating characteristic (ROC) curve was analyzed to identify optimal cut-off criteria (distance in mm, Youden’s index) and determine individual diameter ranges based on aortographic distance measurements of each category of THV sizes. The lowest value from the smallest THV and the highest value from the largest THV was determined using the 25th and 75th IQR, respectively, taken from the distribution of the derivation population. The suggested THV size was derived using aortography with manual or automatic calibration. Sensitivity, specificity, positive, and negative predictive values, as well as positive and negative likelihood were used to determine diagnostic accuracy index. Bland-Altman plots were used to test correlation between the CT NCC-LCC and the NCC-LCC aortography with manual calibration and NCC-LCC aortography with automatic calibration.

Inter- and intra-observer analysis using intraclass correlation coefficient (with absolute agreement) and Pearson correlation coefficient for dichotomized data were performed in a sample of 40 cases between the 2 independent cardiologists.

To perform internal validation, previously established cut-off values to determine THV size by aortography were applied in a separate

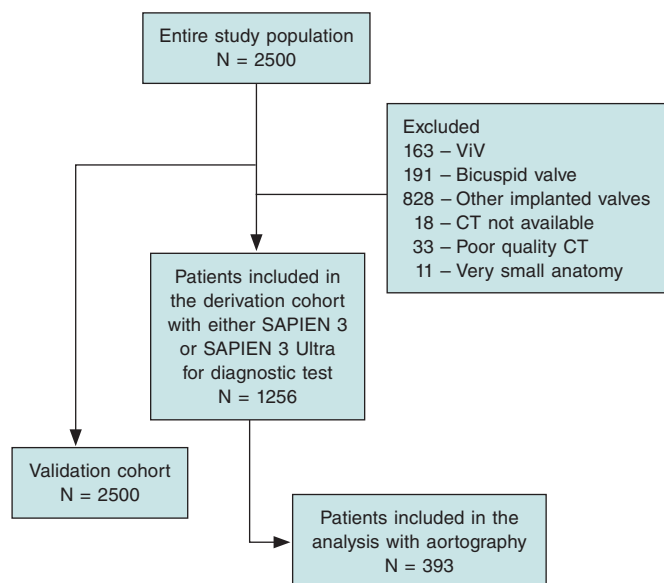


Figure 3. Study enrollment flow diagram.

cohort of 40 patients (validation cohort) and compared using the gold standard CCTA-based sizing determination.

Pairs of sizing results based on angiography and CCTA were generated as a study group of interest and classified as concordant or discordant after comparison using the chi square test or Fischer's exact test, unpaired *t* test or the Mann-Whitney *U* test, as appropriate. Statistical analysis was performed using IBM SPSS Statistics software package (version 27, IBM Corporation, United States). All tests were 2-sided at the 0.05 significance level.

RESULTS

After exclusion, 1256/2500 (50.2%) patients who received a BEV were evaluated in the validation cohort (figure 3). Aortography-based diameter measurements were feasible in 393 of these patients (15.7%) (study group of interest).

Baseline and CCTA characteristics are shown on table 1. The median age of the entire population was 81 (77-85) years, 34.3% female, with a left ventricular function of 60% [47-60], and a median EuroScore II of 3.74 (2.14-6.24).

Procedural characteristics are shown on table 2. Procedural time, fluoroscopic dose, and fluoroscopic time were 48 min [38-59], 919 [444-1712] cGys/cm², and 10.9 min [8.2-14.7], respectively. Technical success was achieved in 95.4% of the cases. Regarding in-hospital complications (table 3), there rates of major bleeding events, major vascular complication, and in-hospital mortality were 16.1%, 14.6%, and 1.5%, respectively.

No differences were reported regarding the efficacy (94.2% vs 96%; *P* = .60) and safety profile (90.9% vs 91.9%; *P* = .84) between discordant and concordant pairs of tomographic and angiographic measurements using aortography with manual calibration, respectively (table 4).

A moderate correlation was seen between CCTA-based assessment and aortographic THV size determination: 23 mm, 26 mm, and 29 mm THV sizes were associated with Spearman's correlation coefficients of 0.528 (*P* < .01), 0.451 (*P* < .01), and 0.579 (*P* < .01), respectively. For more details, see tables 1-3 of the supplementary data.

Table 1. Baseline characteristics

	Balloon-expandable valve (N = 393)
Age, years	81 [77 - 85]
Men	257 (65.7)
BMI, kg/m ²	26.2 [23.8-29.5]
BSA, m ²	1.92 ± 0.22
NYHA functional class III-IV	238 (60.9)
CCS class III-IV	32 (8.2)
Arterial hypertension	353 (90.3)
Diabetes mellitus	131 (33.5)
Dyslipidemia	265 (67.8)
COPD	19 (4.9)
Smoking history	123 (31.5)
PAD	77 (19.7)
Previous PCI	162 (41.4)
CAD	341 (87.2)
1 vessel	204 (52.2)
2 vessels	57 (14.6)
3 vessels	80 (20.5)
Pacemaker implantation	36 (9.2)
Previous MI	43 (11)
Previous CABG	37 (9.5)
Previous Stroke/TIA	60 (15.3)
Atrial fibrillation	149 (38.1)
Creatinine levels, mg/dL	1.11 [0.89-1.37]
eGRF, mL/min	60 [46-76]
Dialysis	3 (0.8)
Aortic regurgitation grade 2+	39 (10)
AVA, mm ²	0.70 [0.60-0.84]
LVEF, %	60 [47-60]
Mean Ao gradient, mmHg	42 [36-49]
Peak Ao gradient, mmHg	68 [59-80]
sPAP, mmHg	42 [33-45]
EuroScore I, %	11.84 [7.82-19.46]
EuroScore II, %	3.74 [2.14 - 6.24]
CCTA measurements	
Minimum diameter, mm	21.6 [20.1-23.2]
Maximum diameter, mm	27.9 [26.2-29.6]
Mean diameter, mm	24.8 [23.2-26.3]
Area, mm ²	474 [414-533]

(Continued)

Table 1. Baseline characteristics (continued)

	Balloon-expandable valve (N = 393)
Perimeter, mm	79 [74-84]
<i>Visual estimate of the severity of valve calcification</i>	
Mild	80 (20.5)
Moderate	185 (47.3)
Severe	126 (32.2)
<i>Visual estimate of the severity of annular calcification</i>	
None	55 (14.1)
Mild	268 (68.5)
Moderate	67 (17.1)
Severe	1 (0.3)
<i>Visual estimate of the severity of LVOT calcification</i>	
None	223 (57)
Mild	145 (37.1)
Moderate	23 (5.9)

Data are expressed as no. (%), mean \pm standard deviation or mean [interquartile range]. Ao, aortic; AVA, aortic valve area; BMI, body mass index; BSA, body surface area; CABG, coronary artery bypass graft; CAD, coronary artery disease; CCS, Canadian Cardiovascular Society angina grading scale; CCTA, coronary computed tomography angiography; COPD, chronic obstructive pulmonary disease; eGFR, estimated glomerular filtration rate; LVEF, left ventricular ejection fraction; LVOT, left ventricular outflow tract; MI, myocardial infarction; mg/dL milligrams per deciliter; mL/min, milliliters per minute; mm², square millimeters; mmHg, millimeters of mercury; NYHA, New York Heart Association functional classification; PAD, peripheral artery disease; PCI, percutaneous coronary intervention; sPAP, systolic pulmonary artery; TIA, transient ischemic attack; %, percentage.

The suggested angiographic cut-off values for each THV size are shown on [table 5](#). In brief, the best diameter range for selecting 23 mm BEVs was 18.46 mm to 22.55 mm; for 26 mm THVs the best diameter range was 21.55 mm to 24.55 mm while for 29 mm THVs the best diameter range was \geq 24.25 mm to $<$ 28.50 mm. The intra- and inter-observer intraclass correlation coefficients were 0.931 (95%CI, 0.869-0.963; $P < .01$), and 0.902 (95%CI, 0.814-0.948; $P < .01$), respectively (see [table 4 of the supplementary data](#)). The CT NCC-LCC distance and NCC-LCC showed an intraclass correlation coefficient of 0.885 (95%CI, 0.834-0.920; $P < .01$) ([figure 4](#)).

The values obtained were tested and compared with the validation cohort (n = 40) showing moderate-to-good diagnostic test analysis with a good Spearman's correlation coefficient [0.711 (95%CI, 0.506-0.840; $P < .01$)], and moderate diagnostic accuracy ([table 5 of the supplementary data](#)). The validation cohort of 40 patients is shown on [tables 6 to 10 of the supplementary data](#).

The 30-day follow-up is shown on [table 6](#). There was no difference in 30-day mortality between discordant and concordant tomographic and angiographic measurements (1.7% vs 2.6%; $P = .73$). There was no difference at 30 days regarding the mean gradient (11 [10-16] vs 12 [10-15] mmHg; $P = .76$), and more than moderate aortic regurgitation (3.2% vs 1.1%; $P = .34$) using aortography with manual calibration between discordant and concordant tomographic and angiographic measurements, respectively.

Table 2. Procedural characteristics

	Balloon-expandable valve (N = 393)
<i>Elective</i>	389 (99.5)
<i>Need for intubation</i>	
Prophylactic	5 (1.3)
Emergency	8 (2)
<i>Use of ECMO</i>	
Prophylactic	0 (0)
Emergency	1 (0.3)
<i>Use of cerebral protection device</i>	16 (4.1)
<i>Size of the valve implanted</i>	
23 mm	118 (30.2)
26 mm	207 (52.9)
29 mm	66 (16.9)
<i>THV implanted</i>	
SAPIEN 3	95 (24.3)
SAPIEN 3 Ultra	296 (75.7)
<i>Predilatation</i>	166 (42.5)
<i>Postdilatation</i>	54 (13.8)
<i>Contrast media, mL</i>	139 [110-172]
<i>Fluoroscopic time, min</i>	10.9 [8.2-14.7]
<i>Fluoroscopic dose, cGys/cm²</i>	919 [444-1712]
<i>Procedural time, min</i>	48 [38 - 59]
<i>Technical success</i>	373 (95.4)
<i>Procedural success</i>	384 (98.2)
<i>Intended performance</i>	380 (97.2)
<i>Correct position</i>	389 (99.5)
<i>Multiple valves</i>	1 (0.3)
<i>Access site complications</i>	18 (4.6)
<i>THV embolization</i>	1 (0.3)
<i>Cardiac tamponade</i>	5 (1.3)
<i>Annular rupture</i>	3 (0.8)
<i>Coronary impairment</i>	0 (0)
<i>Procedural CPR</i>	2 (0.5)
<i>Conversion to surgery</i>	4 (1)
<i>Procedural mortality</i>	3 (0.8)
<i>Angiographic AR \geq moderate</i>	5 (1.3)
<i>Postoperative mean gradient, mmHg</i>	9 [5-10]
<i>Days at the ICU</i>	1 [1-1]

Data are expressed as no. (%), mean \pm standard deviation or mean [interquartile range]. AR, aortic regurgitation; cGys/cm², centigrays per square centimeters, CPR, cardiac pulmonary resuscitation; ECMO, extra corporeal membrane oxygenator; ICU, intensive care unit; THV, transcatheter heart valve; min, minutes; mL, milliliters; mm, millimeters.

Table 3. In-hospital complications

	Balloon-expandable valve (N = 393)
Life-threatening bleeding	11 (2.8)
Major bleeding	63 (16.1)
Minor bleeding	65 (16.6)
Major vascular complications	57 (14.6)
Minor vascular complications	80 (20.5)
TIA	0 (0)
Major stroke	4 (1)
Minor stroke	5 (1.3)
Myocardial infarction	3 (0.8)
New pacemaker implantation	26 (6.6)
In-hospital mortality	6 (1.5)

Data are expressed as no. (%).
TIA, transient ischemic attack.

Table 4. Procedural complications in concordant and discordant valve sizes using manual and automatic calibration in aortography vs CCTA (N = 393)

	All (N = 393)	Discordant (N = 121)	Concordant (N = 272)	P
<i>Efficacy</i>	375 (95.4)	114 (94.2)	261 (96.0)	.60 ^a
Technical success	386 (98.2)	118 (97.5)	268 (98.5)	.44 ^b
Correct position	391 (99.5)	120 (99.2)	271 (99.6)	.52 ^b
Intended performance	382 (97.2)	117 (96.7)	265 (97.4)	.74 ^b
<i>Safety</i>	360 (91.6)	110 (90.9)	250 (91.9)	.84 ^a
Multiple valves	1 (0.3)	0 (0)	1 (0.4)	> .99 ^b
THV embolization	1 (0.3)	0 (0)	1 (0.4)	> .99 ^b
New pacemaker implantation	27 (6.9)	9 (7.4)	18 (6.6)	.83 ^a
AR > moderate after valve implantation	5 (1.3)	2 (1.7)	3 (1.1)	.64 ^b
<i>Conversion to surgery</i>	4 (1.0)	1 (0.8)	3 (1.1)	> .99 ^b
<i>Procedural mortality</i>	3 (0.8)	1 (0.8)	2 (0.7)	> .99 ^b
<i>Life-threatening bleeding</i>	11 (2.8)	5 (4.1)	6 (2.2)	.32 ^b
<i>Major bleeding</i>	64 (16.3)	20 (16.5)	44 (16.2)	> .99 ^a
<i>Minor bleeding</i>	66 (16.8)	16 (13.2)	50 (18.4)	.24 ^a
<i>Major vascular complications</i>	58 (14.8)	17 (14)	41 (15.1)	.87 ^a
<i>Minor vascular complications</i>	81 (20.6)	22 (18.2)	59 (21.7)	.50 ^a
<i>In-hospital mortality</i>	6 (1.5)	2 (1.7)	4 (1.5)	> .99 ^b

Data are expressed as no. (%).
AR, aortic regurgitation; CCTA, coronary computed tomography angiography; no., number; %, percentage.

^a Chi-square test.

^b Fisher's exact test.

Table 5. Suggested angiographic size chart for the SAPIEN balloon-expandable valve

	23 mm	26 mm	29 mm
N-L CC distance	18.46–22.55	21.55–24.55	24.25–28.50

mm, millimeter; mm², square millimeters; N-L CC, non-to-left coronary cusp.

Discussion

This single-center, retrospective, observational study investigated the correlation and diagnostic accuracy between angiographic and tomographic measurements to determine THV size according to 1 single angiographic measurement between the NCC and the LCC in patients treated with BEV.

Regarding this objective, the most salient findings are *a*) angiographic aortic valve annular size determination based on distance measurements between the NCC and LCC is reproducible; *b*) diagnostic accuracy between CCTA-based and angiography-based aortic valve annular size determination is of moderate strength (table 5 of the supplementary data); and *c*) internal validation of previously established diameter ranges for angiography-based aortic valve annular size determination revealed moderate diagnostic accuracy.

We found a moderate overall diagnostic accuracy and correlation between angiographic and CCTA measurements to determine aortic valve annular size for THV selection. The use of angiography only measurements may expand the minimalistic TAVI approach in scenarios where CCTA is not an option or is unavailable.

The gold standard method to size the aortic annulus is direct surgical measurement, which is impossible in the TAVI setting. Hereby, several non-invasive reproducible methods have been used to determine the aortic valve annular size.^{3,5-7,20} However, the CCTA has been established as the gold standard diagnostic tool to determine aortic valve annular size dimensions⁴ due to its outstanding reproducibility. Before CCTA was established as the actual gold standard method, angiographic measurements were used demonstrating good correlation with direct perioperative measurements in patients undergoing surgical aortic valve replacement ($r = 0.93$).¹³ The comparison of transesophageal echocardiography and CCTA and direct perioperative measurements reported by Wang et al.²⁰ showed a moderate correlation. Our study showed moderate diagnostic accuracy and correlation between angiographic and tomographic measurements to determine THV size. Similar results were previously tested in a small sample size of 50 patients where 60% of the valves were properly sized with fair-to-moderate agreement between angiography- and CCTA-guided selections.¹² This provides evidence that angiography measurements could potentially be used in scenarios where CCTA is not available or its application is of increased risk.

Radiation exposure during CCTA assessment

It has been shown that TAVI-related imaging studies can potentially increase radiation exposure by some 15.4 to 79 mSv (millisieverts) with the TAVI procedure alone accounting for an effective dose of 26.9 ± 8 mSv and a dose-area product of 2006.3 ± 1152.2 cGys/cm² (centigrays/cm²). This radiation exposure is associated with a 70% and 50% increased risk of lung cancer-related death in women and men, respectively, and a 12% to 21%, and 23% to 33% risk of leukemia in women and men, respectively.¹⁰ We should mention that our study population experienced lower procedural radiation exposure (919 [444-1712] cGys/cm²) during TAVI including aortic valve annular sizing that may reduce radiation-associated risk of cancer. Using intraoperative low-dose radiation protocols can achieve equal

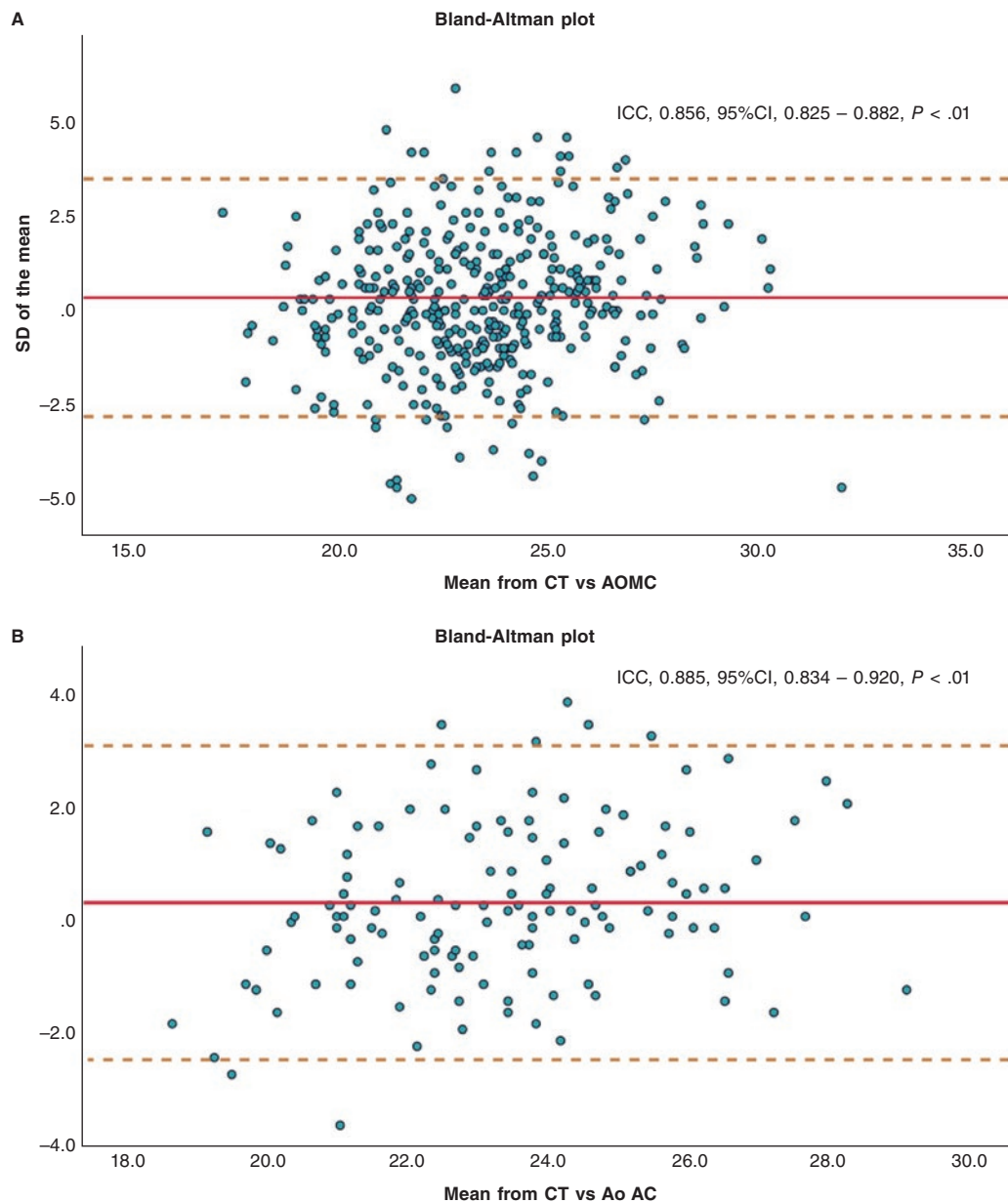


Figure 4. Bland-Altman plots: **A:** CCTA vs AOMC; **B:** CCTA vs Ao AC. Ao AC, aortography with automatic calibration; AOMC, aortography with manual calibration; CCTA, coronary computed tomography angiography; CI, confidence interval; ICC, intraclass correlation coefficient; SD, standard deviation.

efficacy in TAVI patients same as standard protocols without compromising safety,²¹ thus reducing radiation exposure and its associated risk. Additionally, the use of balloon-sizing combined with our proposed angiographic measurements may increase accuracy when determining the necessary THV size. Specifically, when the aortography annular measurement falls near the cut-off value between 2 different THV sizes, balloon-sizing can be used to confirm the use of the larger or smaller device.¹⁵ Although the additional use of balloon-sizing could increase radiation exposure due to additional imaging acquisition, the use of low-dose radiation protocol can reduce this risk without impacting the final result.²¹

Contrast media-associated nephropathy

Besides the benefits of mitigating radiation-associated risks, contrast media-associated nephropathy remains a critical concern in patients

undergoing TAVI. Chronic kidney disease is present in around 38% of patients with aortic valve stenosis, 55%, 30%, and 15% of whom show mild, moderate, and severe chronic kidney disease.²² The use of contrast media can exacerbate acute kidney injury after its administration in patients with moderate-to-severe chronic kidney disease (from 2% to 17%)¹¹ with a higher estimated 5-year mortality rate.²²

Previous studies have demonstrated the safety and efficacy profile of TAVI compared to surgical aortic valve replacement across all ranges of surgical risk.²³⁻²⁸ Against this background, our data suggest that using aortography is safe to facilitate THV size selection in selected indications. In cases where aortography THV sizing was concordant with CCTA determined THV size, the safety and efficacy outcomes reported compared favorably to studies published in similar risk categories of patients.

Table 6. 30-day follow-up comparing concordant vs discordant measurements using balloon-expandable valve

	Total (N = 393)	Discordant (N = 121)	Concordant (N = 272)	P
Mortality	9 (2.3)	2 (1.7)	7 (2.6)	.72 ^a
CHF	24 (6.1)	8 (6.6)	16 (5.9)	.82 ^b
Stroke	2 (0.5)	0 (0)	2 (0.7)	> .99 ^a
Valve dysfunction	8 (2)	2 (1.7)	6 (2.2)	> .99 ^a
LVEF, %, (n 278)	60 [60-60]	60 [57-60]	60 [50-60]	< .01 ^c
Mean gradient, mmHg (n = 265)	12 [10-15]	11 [10-16]	12 [9.8-15]	.76 ^c
AR > moderate, (n = 279)	5 (1.8)	3 (3.2)	2 (1.1)	.33 ^a
NYHA ≥ III, (n = 345)	18 (5.2)	5 (4.6)	13 (5.5)	.80 ^a

Data are expressed as no. (%), mean ± standard deviation or mean [interquartile range]. AR, aortic regurgitation; CHF, congestive heart failure; LVEF, left ventricular ejection fraction; mmHg, millimeters of mercury; NYHA, New York Heart Association functional class.

^a Fisher's exact test.

^b Chi-square test.

^c Mann-Whitney U test.

Study limitations

This study is limited by its single-center observational nature. A randomized or prospective study may be needed to confirm our results. Furthermore, the use of 1 type of fluoroscopy equipment may limit the applicability of the findings to fluoroscopy equipment from alternative manufacturers. Additionally, due to data storage limitations, angiography was not always available to determine the aortic valve annular size through manual or automatic calibration. Upper and lower values of the suggested size chart were determined based on 75th and 25th interquartile range, respectively, due to the lack of upper or lower outliers that would allow us to determine these values.

CONCLUSIONS

Angiographic aortic valve annular measurements are reproducible and show moderate correlations and diagnostic accuracy compared to CCTA measurements when selecting the proper BEV THV size. This technique may be appropriate in situations when CCTA is not available, when high radiation exposure needs to be avoided, for patients in critical condition, and to reduce the risk of contrast-induced nephropathy. This strategy could potentially advance the minimalistic TAVI approach in selected patients.

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AUTHORS' CONTRIBUTIONS

H. A. Alvarez-Covarrubias: conceptualization, methodology, formal analysis, investigation, resources, and original drafting of the manuscript. M. Kasel: conceptualization, original drafting of the manuscript, and editing. J.M. Michel: original drafting of the manuscript, and formal analysis. S. Cassese: visualization, investigation. S. Kufner: supervision, and data curation. C. Duesmann, C. Pellegrini, T. Rheude, and N. P. Mayr: resources, and data curation. H. Schunkert: supervision, drafting and revision of the manuscript, and visualization editing. A. Kastrati: supervision, visualization,

drafting and revision of the manuscript, and editing. E. Xhepa: drafting of the manuscript, supervision, and formal analysis. G. Borraro-Sánchez, and M. Joner: conceptualization, drafting and revision of the manuscript, and project administration.

CONFLICTS OF INTEREST

M. Kasel reports being a proctor and consultant for Edwards Lifesciences, but totally unrelated to this study; J. M. Michel reports a being proctor for Boston Scientific, but totally unrelated to this study; S. Cassese reports having received grants from Abbott Vascular, Boston Scientific, and SIS Medical AG, consulting fees from SIS Medical AG, and speaker fees from Abiomed, Astra Zeneca, SIS Medical AG, and Teleflex, but totally unrelated to this study; S. Kufner reports having received speaker and consultant fees from AstraZeneca, Bristol Myers Squibb, Bentley, and Translucina, but totally unrelated to this study; C. Pellegrini reports having received a grant from Else-Kröner Fresenius Memorial Stipendium, but totally unrelated to this study; T. Rheude reports having received lecturer fees from SIS Medical AG, and Astra Zeneca, but totally unrelated to this study; H. Schunkert reports having received consulting, honoraria, and speaker fees from AMGEN, Daiichi-Sankyo, MSD SHARP&DOHME, Astra Zeneca, Bayer Vital, Boehringer-Ingelheim, Novartis, Servier, and Synlab, but totally unrelated to this study; A. Kastrati reports a patent number PCT/EP2021/053116, and participation on the Data Safety Monitoring Board of the DSMB-TARGET Trial, but totally unrelated to this study; E. Xhepa reports having received lecturer and speaker fees from Astra Zeneca, Boston Scientific, and SIS Medical AG, and support for attending meetings from Abbott Vascular, but totally unrelated to this study; G. Borraro reports being former president of the Asociación Nacional de Cardiólogos de México from 2020 through 2022; M. Joner reports having received grants from Boston Scientific, Cardiac Dimensions, Edwards Lifesciences, Infraredx, consulting fees from Biotronik, TriCares, Veryan and Shockwave, and lecturer and speaker fees from Abbott Vascular, Biotronik, Boston Scientific, Edwards Lifesciences, Cardiac Dimensions, Astra Zeneca, Recor Medical, and Shockwave, but unrelated to this study; the remaining authors declared no conflicts of interest whatsoever. This manuscript is part of the Masters and PhD program in medical sciences of Universidad Nacional Autónoma de México (UNAM).

WHAT IS KNOWN ABOUT THE TOPIC?

- Little has been investigated in relation to the implementation of aortography as a diagnostic test to determine aortic valve annular size.
- Former studies used aortography to determine balloon size in valvuloplasty treatment in the pre-TAVI era.
- Aortography has been used in the TAVI era as a method to determine annular plane and for valve delivery purposes.

WHAT DOES THIS STUDY ADD?

- Implementation of aortography in addition to coronary computed tomography angiography (CCTA) may help us decide the size of the valve where gray zones areas are seen on the CCTA.
- Aortography measurements are reproducible and give moderate accuracy to decide the size of the valve in cases where CCTA is not available, and patients must be treated immediately.

SUPPLEMENTARY DATA



Supplementary data associated with this article can be found in the online version available at <https://doi.org/10.24875/RECICE.M23000367>.

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